Optical Response to LASIK Surgery for Myopia from Total and Corneal Aberration Measurements

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PURPOSE. To evaluate the optical aberrations induced by LASIK refractive surgery for myopia on the anterior surface of the cornea and the entire optical system of the eye.

METHODS. Total and corneal aberrations were measured in a group of 14 eyes (preoperative myopia ranging from −2.5 to −13 D) before and after LASIK surgery. Total aberrations were measured using a laser ray-tracing technique. Corneal aberrations were obtained from corneal elevation maps measured using a corneal system and custom software. Corneal and total wave aberrations were described as Zernike polynomial expansions. Root-mean-square (RMS) wavefront error was used as a global optical quality metric.

RESULTS. Total and corneal aberrations (third-order and higher) showed a statistically significant increase after LASIK myopia surgery, by a factor of 1.92 (total) and 3.72 (corneal), on average. This increase was more pronounced in patients with the highest preoperative myopia. There is a good correlation (r = 0.97, P < 0.0001) between the aberrations induced in the entire optical system and those induced in the anterior corneal surface. However, the anterior corneal spherical aberration increased more than the total spherical aberration, suggesting also a change in the spherical aberration of the posterior corneal surface. Pupil centration and internal optical aberrations, which are not accounted for in corneal topography, play an important role in evaluating individual surgical outcomes.

CONCLUSIONS. Because LASIK surgery induces changes in the anterior corneal surface, most changes in the total aberration pattern can be attributed to changes in the anterior corneal aberrations. However, because of individual interactions of the aberrations in the ocular components, a combination of corneal and total aberration measurements is critical to understanding individual outcomes, and by extension, to designing custom ablation algorithms. This comparison also reveals changes in the internal aberrations, consistent with the posterior corneal changes reported using scanning slit corneal topography. (Invest Ophthalmol Vis Sci. 2001;42:3349–3356)

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23 days) LASIK surgery. The preoperative spherical refractive error ranged from $-2.5$ to $-13$ D (mean, $-6.8 \pm 2.9$ D), and preoperative astigmatism was less than 2.5 D. Postoperative recovery was uneventful, and none of the patients was retreated. The procedures were reviewed and approved by institutional bioethics committees and met the tenets of the Declaration of Helsinki. All patients were fully informed and understood and signed an informed consent before enrollment in the study. Aberration measurements were conducted at Instituto de Optica, Consejo Superior de Investigaciones Científicas (CSIC), Madrid, Spain. Generally, both types of measurements (total and corneal aberrations) were obtained bilaterally in one experimental session.

**LASIK Surgery**

Standard LASIK surgery was conducted using a narrow-beam, flying-spot excimer laser (Chiron Technolas 217-C equipped with the PlanoScan program; Bausch & Lomb Surgical, Madrid Spain). This laser has an emission wavelength of 193 nm, a fixed pulse repetition rate of 50 Hz, and a radius exposure of 400 mJ. The procedure was assisted by an eye tracker. The flap diameter (performed with a Hansatome microkeratome; Bausch & Lomb España, SA, Madrid Spain) was 8.5 mm, and the intended depth was 180 μm. Photoablation was applied to a 6-mm optical zone, with a transition zone of 9 mm. The LASIK procedures were conducted at the Instituto de Ofalmobiología Aplicada, Universidad de Valladolid, Spain.

**Total Aberrations Using LRT**

Total wave aberrations were measured using laser ray tracing (LRT), developed at the Instituto de Optica in Madrid, Spain.12 The principles and, in particular, its use as an evaluation tool in LASIK surgery for myopia, have been described in detail elsewhere.18 In this technique, a scanning system scans a narrow laser beam (543 nm) across the pupil. Simultaneously, a high-resolution charged-coupled device (CCD) camera captures the retinal spot images corresponding to each entry pupil location. Figure 1A shows a particular series of images after surgery in a LASIK-treated eye. The positions of the centroids of the set of retinal images form a spot diagram (Fig. 1B). The deviations of each centroid from the principal ray are proportional to the local slopes of the wave aberration. Each run consists of 37 rays, sampling a 6.5-mm pupil in 1-mm steps in a hexagonal pattern, and lasts 4 seconds. Each measurement is repeated five times.

Aberration measurements were obtained after pupil dilation with 1 drop tropicamide 1%. Subjects' heads were stabilized with a dental impression and a headrest, and the pupil was continuously monitored on a CCD camera to ensure proper alignment of the pupil center to the optical axis of the instrument. Spherical refractive errors were corrected with trial lenses when necessary. The raw data (derivatives of the wave aberration) were fitted to a seventh-order Zernike ($Z$) polynomial, and the wave aberration was obtained using a least-mean-squares procedure. We used the root-mean-square (RMS) wavefront to assess global optical quality and its change with LASIK. We analyzed either individual Zernike ($Z$) terms (i.e., $Z_{20}$, spherical aberration) or the RMS for third-order terms and higher, i.e., including piston ($Z_{20}$), tilt ($Z_{21}$ and $Z_{22}$), defocus ($Z_{40}$), and astigmatism ($Z_{22}$ and $Z_{21}$), and for isolated $Z$ terms. In these group of patients, Zernike coefficient SD (averaged across terms) ranged from 0.026 to 0.170 μm (mean, 0.069 ± 0.037 μm [SD]).

**Corneal Aberrations from Corneal Topography**

Corneal height numerical data were obtained with a corneal topography system (Atlas Mastervue; Humphrey Instruments-Zeiss, San Leandro, CA). These data were processed using custom software (Matlab; Mathworks, Natik, MA) and exported to an optical design program (Zemax ver. 9; Focus Software, Tucson, AZ), which performed a ray-tracing simulation to compute corneal aberrations from corneal topography data.32–35 This technique has been validated in recent studies of keratoconus and aphakia.36 Both the corneal surface and the corneal aberration pattern (at the plane of best focus) were described by a Zernike polynomial expansion. We checked that a seventh-order polynomial expansion represented a good description of the surface: the RMS error of the fitting was $0.43 \pm 0.11$ before surgery and $0.53 \pm 0.11$ after surgery (average across the eyes of this study). This error is lower than the accuracy of the corneal topography devices, which can measure surfaces to an RMS error of $3.7 \pm 0.7 \mu m$.37

Figure 1C shows a corneal elevation map (10-mm diameter, centered on the corneal reflex) for the same eye as in Figure 1A. To show the irregularities, we subtracted the first six terms of a Zernike polynomial fit to the height data from the raw height data.34 Ray aberrations were obtained by virtual ray tracing, sampling $64 \times 64$ points of the corneal surface (in a rectangular grid). Figure 1D shows a spot diagram corresponding to a subset of 91 rays, through a 6.5-mm corneal region centered at $-0.6$ to $+0.6$ mm from the corneal reflex. The indices of refraction were taken as that of the air and the aqueous humor (1.3391). For this analysis, the corneal index of refraction was not considered. Wavelength was set to 543 nm (as in the LRT measurements). Unlike the LRT measurements (for which the reference was the pupil center), corneal topography typically uses the corneal reflex (location of the first Purkinje image when the subject fixates foveally) for alignment. Proper alignment of corneal and total aberration is necessary for direct comparison.

We developed custom software to locate the colinear pupil position.36 Corneal aberrations were computed over a large pupil diameter (10 mm) and recomputed over a 6.5-mm pupil (matching the pupil size of total aberration measurements), moving the center over a
±1-mm grid, in 0.1-mm steps. A difference total-corneal map was computed for each pupil location. These maps were smooth and in all cases showed a clear, single minimum—typically, slightly decentered from the corneal reflex. Despite the underlying assumptions, independent observations in control subjects showed that this procedure identifies well the pupil center (inaccessible otherwise from the corneal topography images). Apart from the decentration between the corneal reflex and pupil center, the keratometric axis is tilted with respect to the line of sight. This angle can be computed by measuring the distance between the corneal intersect of the keratometric axis and corneal sighting center (not available in our patients) and using the fixation point distance. Mandell reported an average difference of 0.38 ± 0.10 mm between the corneal intersect of the keratometric axis and the corneal sighting center across 20 normal eyes. Assuming similar values in our group of eyes and for the 148.3-mm fixation point distance in our videokeratoscope, the neglected corneal tilt is approximately 0.15°. For a typical cornea (eye 10) we found that, considering this tilt, RMS changes by only 2.7% before surgery and 0.68% after surgery for third-order \( Z \) terms and by 0.96% before surgery and 0.15% after surgery for spherical aberration (\( Z^4 \)).

In this particular experiment, we obtained only one corneal map per eye and per session. Experiments in one control eye (RMS = 0.59 μm, for third- and higher order terms) showed a Zernike coefficient SD of 0.016 (averaged across terms). Experimental centration errors (SDs) were 0.08 mm for the horizontal coordinate and 0.08 mm for the vertical coordinate.

RESULTS

Total and Corneal Wave Aberration Patterns

Figure 2 shows contour plots of wave aberration patterns for total and corneal aberrations before and after LASIK surgery, in six eyes. Piston, tilts, defocus, and astigmatism have been excluded in all cases, so that these patterns represent simulated best corrected optical quality. Pupil diameter is 6.51 mm, and contour lines are plotted every 1 μm. There was a clear deterioration (accounting for an increase in the number of contour lines) after surgery, both for total and corneal aberrations. Before surgery, total and corneal aberrations showed similarities in only some of the eyes, whereas after surgery, total and corneal aberrations showed very similar patterns, indicating the prevalence of corneal defects over the entire optics. LASIK induced a round central area (with various amounts of decentration, depending on the eye) of positive aberration, surrounded by an area of negative aberration.

Comparison of the Change in Total and Corneal Aberrations with LASIK

RMS wavefront error increased with LASIK, both for total and corneal aberrations. Figure 3 shows RMS before and after LASIK for third- and higher order aberrations—that is, best corrected for defocus and astigmatism. Figure 3A shows the change for total aberrations and Figure 3B the change for corneal aberrations. The eyes were sorted by increasing preoperative spherical error. Before surgery, total aberrations tend to increase with myopia, although this tendency was not evident in corneal aberrations. Both total and corneal aberrations increased significantly after LASIK, except for eyes 5 and 6 for total aberrations, and eye 4 for corneal aberrations. Clearly, for both total and corneal aberrations the increase was much more pronounced in the most myopic eyes.

Total aberrations increased on average by a factor of 1.92 and corneal aberrations by a factor of 3.72. For the low pre-
operative myopia group (−2.5 to −6.5 D) the average increase was 1.53 (total) and 1.97 (corneal), whereas for the high preoperative myopia group (−6.8 to −13.1 D) the average increase was 2.29 (total) and 4.37 (corneal). In terms of RMS differences (before minus after surgery), total RMS difference changed from −0.05 to 0.80 μm, reaching statistical significance in 11 of the 14 eyes, and corneal RMS changed from −0.16 to 2.04 μm, statistically significant in 13 of the 14 eyes. Part of this increase is accounted for by an increase in the third-order aberrations (increasing by a factor of 1.98 for total and 2.73 for corneal) and by an increase of the fourth-order aberrations (increasing by a factor of 2.54 for total and 3.95 for corneal).

Figure 4 shows the change of the fourth-order spherical aberration coefficient ($Z_4^0$), both total (Fig. 4A) and corneal (Fig. 4B). Sign and normalization follow the convention suggested by the Optical Society of America Standardization Committee. The preoperative total spherical aberration coefficient was close to zero in most eyes (significantly positive in seven eyes and significantly negative in three eyes). Preoperative corneal spherical aberration was positive in all eyes, except for one that was not significantly different from zero. Total spherical aberration increased significantly with LASIK in all eyes and corneal spherical aberration in all but one eye. The most dramatic increase occurred in patients with the highest preoperative myopia, both for total and corneal aberrations. Total spherical aberration $Z_4^0$ coefficient for the pre-minus postoperative difference ranged from 0.22 to 1.64 μm (0.63 μm, on average), and for the cornea the differences ranged from −0.01 to 1.72 μm (0.74 μm on average). The increase of spherical aberration seems to be more pronounced for corneal than for total aberrations.

Figure 5 shows post-LASIK corneal versus total aberrations, Figure 5A for third-order and higher aberrations and Figure 5B for RMS for spherical aberration (i.e., roughly the modulus of the data in black bars in Fig. 4, although not exactly, because it includes the contribution of $Z_6^0$ also). There was a very good correlation between corneal and total aberrations (third-order and higher) after LASIK ($r = 0.97$, $P < 0.0001$; slope = 1.01; Fig. 5A). The corneal spherical aberration after LASIK was also well correlated to the total spherical aberration after LASIK ($r = 0.91$, $P < 0.0001$; slope = 1.22; Fig. 5B). However, that the slope is significantly higher than 1 suggests that a larger spherical aberration is induced in the anterior corneal surface than in the entire eye. A higher slope in the post-LASIK corneal versus total aberration was
found for the RMS of the spherical aberration, the spherical aberration coefficient \( Z^s \), and the RMS of fourth-order \( Z \) terms, but not for third-order aberrations or all high-order aberrations (third-order and higher).

**Change of Internal Aberrations with LASIK**

The internal aberrations can be computed by subtracting corneal from total aberration coefficients. Figure 4C shows the internal aberrations before and after LASIK. We found that internal spherical aberration changed significantly in 10 eyes after LASIK. Except for the four less myopic eyes (eyes 1-4) and eye 10, the internal spherical aberration changed toward more toward the negative. Experiments performed in control subjects who had undergone a surgical procedure performed in two different experimental sessions (separated by at least 1 month, as in the surgical eyes) did not reveal statistically significant changes in the internal aberrations across sessions. This indicates that possible changes across sessions in the accommodative state or decentrations of corneal topography terms (which also changed with decentration) are excluded in the internal aberration data. According to our computations, corneal aberration data (third-order and higher) changed by 10% when the pupil position was taken into account. Although, as expected, spherical aberration did not change significantly by recentration (3% on average), third-order aberrations changed by 22%

**Role of Pupil Centration**

Several studies have shown the impact of refractive surgery for myopia (radial keratotomy [RK] and photorefractive keratectomy [PRK]) on corneal aberrations. As in the present analysis, those studies computed the corneal aberration pattern by measuring corneal elevation maps using commercial corneal videokeratoscopes. In these devices, centration is typically achieved by aligning a set of concentric rings to the corneal reflex of the fixation light. Corneal aberrations are then typically referred to the corneal reflex rather than the pupil center. The position of the pupil is important for a correct estimation of retinal image quality and should be taken into account when predicting visual performance from corneal aberration data. According to our computations, corneal aberration data (third-order and higher) changed by 22%.

**Role of Preoperative Internal Optics**

Total aberrations result from the combination of corneal and internal aberrations and their inter-relationships. Before surgery, both components contributed comparable amounts of
aberrations—in some cases even balancing each other. Figure 2 shows that whereas before surgery the cornea dominated the total wave aberration pattern in some eyes (i.e., eye 1 or 7), in some others there was little similarity between total and corneal patterns, indicating an important contribution of the internal optics. Although the relative contribution of the internal optics is expected to be much lower after refractive surgery, interactions between corneal and internal optics may still play some role in determining the surgical outcomes. A recent study indicates a high degree of balance between corneal and internal aberrations in normal young eyes. Before surgery, we found a term-by-term balance of at least 50% of the aberration in 28% of the 14 eyes of this study. For spherical aberration, this balance increased to 57% of the eyes. In 78% of the eyes, the spherical aberration of the anterior corneal surface and the internal optics had a different sign (Fig. 4, white bars).

Furthermore, it is not uncommon (35%) that the amount of negative internal spherical aberration (likely from the crystalline lens) exceeds the amount of positive spherical aberration of the anterior corneal surface. Figure 8 illustrates one of these cases (eye 6), with a corneal preoperative spherical aberration \(Z_2^2\) of 0.38 μm and internal preoperative aberration of −0.48 μm. The upper row shows the measured total and corneal and the computed internal aberration patterns. The negative internal aberration dominates the central area total aberration pattern. After LASIK (lower row), positive spherical aberration is induced on the anterior corneal surface, which cancels (actually overcompensates) the preoperative negative spherical aberration of the internal optics. For this reason, the post-LASIK total aberration pattern for this eye is much better than predicted from corneal aberrations alone. Unlike other subjects with similar preoperative myopia and similar corneal topography after LASIK, this subject did not show any loss of contrast sensitivity (actually improved at two spatial frequencies).

An individual comparison of pre- and postsurgical total and corneal aberration can be invoked to explain the surprisingly good surgical outcomes in this patient. In general, the possible balance between corneal and internal aberration gets disrupted with refractive surgery. In our study, compensation of more than 50% of the corneal spherical aberration by the preoperative internal aberrations decreased from eight eyes before surgery to four eyes after surgery and only happened in eyes with the lowest preoperative spherical errors (eyes 2, 3, 5, and 6). However, at least in these eyes, these interactions are relevant in determining the total wave aberration pattern.

**LASIK-Induced Posterior Corneal Aberrations and Biomechanical Response**

Comparison of post-LASIK corneal and total aberrations revealed an increase in the amount of negative internal spherical aberration, which tended to slightly attenuate the impact of the positive spherical aberration induced in the anterior corneal surface (Fig. 6). The effect was larger as the preoperative spherical refractive error increased and did not depend on the preoperative internal aberrations. The correlation coefficient of post-LASIK internal spherical aberration to pre-LASIK spherical refractive error is 0.73 \((P = 0.0024)\) and of the induced internal spherical aberration (before minus after surgery) to pre-LASIK spherical refractive error is 0.74 \((P = 0.0016)\). LASIK surgery is not likely to induce changes in the crystalline lens; the changes therefore seem to occur in the posterior corneal surface. The effect is only present for spherical aberration, but not for other terms.

This finding is consistent with recent reports using scanning slit corneal topography. They show posterior corneal surface changes of curvature after PRK for myopia and LASIK, which produce a forward shift of the posterior corneal surface. This suggests that after LASIK and PRK the thinner, ablated cornea may bulge forward slightly, steepening the posterior corneal curvature. This effect has been thought to account for the regression toward myopia that is sometimes found after treatment, particularly in the patients with highest preoperative myopia. We used a simple corneal model with aspherical surfaces and found that the observed mean changes of internal spherical aberrations are consistent with the changes in power and asphericity of the posterior corneal surface that have been reported recently. Seitz et al. found that the posterior central corneal power changed significantly from \(-6.28\) to \(-6.39\) D after LASIK, and the asphericity power changed from \(0.98\) to \(1.14\), in a group of eyes with preoperative spherical refractive error similar to those in our study (range: \(-1.00\) to \(-15.50\), mean, \(-5.07 \pm 2.81\) D). For these data, we found that the
induced spherical aberration of the posterior corneal surface is $-0.103 \, \mu m$—very similar to the change in internal spherical aberration that we measured experimentally ($-0.110 \, \mu m$, on average).

In summary, using a combination of aberrometry and anterior corneal topography, we showed that this change in the posterior corneal shape also produced a decrease of spherical aberration in comparison with that predicted from anterior corneal aberrations alone. Our results confirm that this biomechanical corneal response is correlated with the amount of preoperative myopia (or, equivalently, with the depth of corneal ablation). From previous studies, it is likely that it also depends on the preoperative corneal thickness and intraocular pressure.

**Implications**

Our results have important implications for the evaluation outcomes in standard LASIK surgery for myopia, as well as for the design of wavefront-guided ablation procedures (designed to individual canceling preoperative aberrations). First, the results show that the combination of corneal and total aberrations is necessary to understand individual surgical outcomes and their impact on visual performance. In general, both corneal and total aberrations increased with surgery, but the particular increment depended on the individual subject. This is particularly critical in any aberration-free procedure, which cannot rely on the mean population response, but must be adapted to the individual patient. Second, total wavefront aberration measurements complement corneal topography information to gain insight into the biomechanical corneal response. Although the ablation is applied on the anterior corneal surface, our analysis revealed changes in the shape of the posterior corneal surface, assessed by the modification of its spherical aberration.

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